C W_{Let} : Division; Dynamic light scattering; Micelles; Monomers

Analytical & Bioanalytical Techniques ^rna^l ^o^f ^Ana^l^y

Introduction

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Solute molecules associate via a variety of mechanisms driven by molecular and ionic interactions. Examples of these mechanisms are polymerization, aggregation, and the formation of micelles [1-5]. e diusion of such solutes has been the subject of many studies and has proven to be a useful measure of the strength and nature of these interactions.

Mutual di usion coe cients and interaction parameters can be measured for associating solutes via a range of methods including dynamic light scattering (DLS), which is a well-established method, and Taylor dispersion analysis (TDA), which is relatively new. e latter can be achieved via concentration titration methods [6-9] or from a single measurement [10]. Mutual di usion refers to the uxes of solute and solvent molecules produced by changes or gradients in the concentration of the solution. Furthermore, the concentration dependence of mutual di usion coe cients is widely used to characterize the behavior of molecules in solution and, in particular, to identify conditions where molecular interactions are most favorable in terms of stability. is is because typically, the strengths of these interactions become more pronounced with increasing solute concentration as the solution tends to non-ideality [10], thereby leading to a dependence of the diusion coe cient on solute concentration. is is of great importance in the development of biopharmaceutical drugs [11-13] where it can be used to determine the second virial coe $\,$ cient $(B_2^{\,})$, which is a measure of the strength of protein-protein interactions for example.

e di usion interaction parameter, $k_{\rm\scriptscriptstyle D}$ is a metric that describes the variation of a binary diusion coecient with solute concentration in a given medium and is dened by:

 $D^m = D_0(1 + k_D C)$ (1) where D^m is the measured mutual di usion coe cient at a **Citation:** (2016) Theoretical Comparisons of the Concentration-Dependent Diffusion Coefficients from Dynamic Light Scattering and

Taylor Dispersion Analysis. J Anal Bioanal Tech 7: 340. doi: 10.4172/2155-9872.1000340

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From Eq. (3),

$$
c_i' \quad iK_i c_1^{i-1} \quad c_1(i-1) \tag{9}
$$

which gives

$$
\int_{i=1}^{n} i^{2} K_{i} c_{1}^{i} D_{i} c_{1}^{j} D_{l}^{m} \frac{1}{i^{2}} K_{i} c_{1}^{i} c_{1}^{j} c_{1}^{j}
$$
 (10)

where K_{1} =1.

Dividing by c_1 and re-arranging with the aid of Eq. (3) gives

$$
D^{m} \quad \frac{\sum_{i=1}^{n} i^{2} c_{i} D_{i}}{\sum_{i=1}^{n} i^{2} c_{i}} \quad \frac{1}{\left| \sum_{i=1}^{n} i^{2} K_{i} c_{i}^{i} D_{i} \right|} \tag{11}
$$

Henceforth, this will be referred to as the intrinsic mutual diusion coe cient.

$$
\mathcal{L}_{\mathcal{A}}(t_{1\textbf{q}},\lambda), A_{\textbf{q}}(t_{1},\lambda_{1},\mu_{1},\mu_{1},\mu_{1}^{e})
$$

For DLS, each D_i is weighted by the product of the mass concentration *C*_i and mass m_i . Hence the weight factor is m_i^2 . is is proportional to $i^2 c_i^2$. erefore, for a DLS measurement, Eq. (11) can becomes weighted as follows:

$$
D_{\text{DLS}}^m \quad \frac{\prod_{i=1}^n i^4 c_i^3 D_i}{\prod_{i=1}^n i^4 c_i^3} \prod_{i=1}^n \frac{\prod_{i=1}^n i^4 (K_i c_i^i)^3 D_i}{\prod_{i=1}^n i^4 (K_i c_i^i)^3}
$$
(12)

For TDA, where the dispersion of a plug of solute within a capillary is monitored as a function of time, it is the dispersion coe cient *d* that is determined using the form of Eq. (11) i.e.,

$$
\frac{\frac{n}{i} \mathbf{1}^{2} \mathbf{c}_{i} \mathbf{d}_{i}}{\frac{n}{i} \mathbf{1}^{2} \mathbf{c}_{i}} \frac{\frac{n}{i} \mathbf{1}^{2} \mathbf{K}_{i} \mathbf{c}_{i}^{i} \mathbf{d}_{i}}{\frac{n}{i} \mathbf{1}^{2} \mathbf{K}_{i} \mathbf{c}_{1}^{i}}
$$
(13)

e mutual diusion coecient *D*^m is obtained from the dispersion coe cient via the reciprocal relation [18]:

$$
d \quad \frac{r^2v^2}{48D^m} \tag{14}
$$

where

d

$$
d_{\text{TDA}} \quad \frac{\sum_{i=1}^{n} i^{3} c_{i}^{2} d_{i}}{\sum_{i=1}^{n} i^{3} c_{i}^{2}} \prod_{i=1}^{n} \frac{i^{3} (K_{i} c_{i}^{i})^{2} d_{i}}{\sum_{i=1}^{n} i^{3} (K_{i} c_{i}^{i})^{2}}
$$
(15)

is the capillary radius and ν is the average ow speed. For a massconcentration sensitive instrument, the dispersion coe cients *d* are weighted by m_i (ic_i), hence for TDA, the weighted dispersion coe cient becomes. is gives:

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Note that $K_{2}c_{1}=c_{2}$ from Eq. (3).

It is also instructive to investigate the behavior of the interaction parameter. e interaction parameter, which is dened in Eq. (1), may be estimated from the rst derivative of the diusion coecient with respect to concentration and is given by:

$$
k_{D} \quad \frac{1}{\cdot} \frac{dD^{m}}{dD}
$$

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all three interaction parameters tend to zero. ese observations are better appreciated by expanding the expressions for the interaction parameters in these limits. At low concentrations, they reduce to:

$$
\begin{aligned} k_{\mathrm{D}} & \overset{\text{C00}}{=} 4K_2 \frac{(\boldsymbol{D}_2 - 4\boldsymbol{\xi})\boldsymbol{\delta}}{\boldsymbol{D}_1} \\ k_{\mathrm{D}}^{\mathrm{DLS}} & \overset{\text{C00}}{=} 48K_2^3 c_1^2 \frac{(\boldsymbol{D}_2 - \boldsymbol{D}_1)}{\boldsymbol{D}_1} \\ k_{\mathrm{D}}^{\mathrm{TDA}} & \overset{\text{C00}}{=} 16K_2^2 c_1 \frac{(\boldsymbol{D}_2 - \boldsymbol{D}_1)}{\boldsymbol{D}_2} \end{aligned}
$$

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Intrinsic DLS TDAFigure 6:

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